## Almost-Impossible Materials Science by 3D Diffraction Microscopy

Ian McNulty

**BESSY / Advanced Photon Source** 





## Outline



**Motivation** 

**Resolution and 3D** 

**Coherent methods** 

The need for speed

**Future directions** 

## The challenge



- The capability to image structure in 3D at the molecular scale and beyond is essential to solve many problems in materials science
- Electron microscopes, STMs, AFMs, etc., are superb tools but are limited to surfaces and thin films
- X-ray crystallography is not, but depends on crystalline samples
- Lenses limit the resolution of conventional x-ray microscopes, and 3D methods are impractically slow for many experiments.



How can we reach beyond these limits?

We need better tools to study ordering



Figure 1. Typical length scales and dimensionality of disorder in some classes of materials. The disorder in most materials is usually defined relative to a lattice. Glasses are an exception, where short range order is determined by nearest neighbour bond distances and interbond angles.

M. Treacy et al., Rep. Prog. Phys. 68, 2899 (2005)

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Aerogels form interconnected networks



### A.. Roshi, S. Barjami, G. lannacchione (Worchester Polytechnic Inst.)

Aerosils and gels form long, necklacelike, chains that interconnect randomly and percolate with fractal dimensions. Dynamics and fluctuations are modified by phase transitions in surrounding matrix (e.g., smecticphase liquid crystal)



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### **Materials Science and Engineering**



### Block Copolymer directed Hybrids in Bulk



TEM

R. Ulrich, A. Du Chesne, M. Templin, U. Wiesner, Adv. Mater. 11, 141 (1999)

Cr antiferromagnetic domain evolution



### Diffraction contrast shows regions with different magnetic order



# Spin-flip transition T<sub>SF</sub> is non-uniform within domain

P. Evans et al., *Science* 295, 1042 (2002) Need brilliance to get intense, small spot





| Modes:  | Short-Term Goals |                        |                        | Long-Term Goals              |                              |         |
|---|------------------|------------------------|------------------------|------------------------------|------------------------------|---------|
|   | (A)<br>Flux      | (B) High-<br>Coherence | (C)<br>Short-<br>Pulse | (D) Ultra High-<br>Coherence | (E) Ultra<br>Short-<br>Pulse | Unit    |
| Energy  | 5                | 5                      | 5                      | 5                            | 5                            | GeV     |
| Macropulse current                              | 100              | 25                     | 1                      | 100                          | 1                            | mA      |
| Bunch charge                                    | 77               | 19                     | 1000                   | 77                           | 10000                        | рС      |
| Repetition rate                                 | 1300             | 1300                   | 1                      | 1300                         | 0.1                          | MHz     |
| Transverse emittance<br>(norm. rms)             | 0.3              | 0.08                   | 5.0                    | 0.06                         | 5.0                          | mm.mrad |
| Transverse emittance<br>(geometric at 5GeV)     | 31               | 8.2                    | 511                    | 6.1                          | 511                          | pm      |
| Bunch length (rms)                              | 2000             | 2000                   | 50                     | 2000                         | 20                           | fsec    |
| intrabunch Energy<br>spread<br>(fractional;rms) | 2E-4             | 2E-4                   | 3E-3                   | 2E-4                         | 3E-3                         |         |
| Beam power                                      | 500              | 125                    | 5                      | 500                          | 5                            | MW      |
| Beam loss                                       | < 1              | < 1                    | < 1                    | < 1                          | < 1                          | μA      |

Image formation as a scattering process



Ewald sphere (2D) defined by conservation of momentum and limit of spatial frequencies in the object defined by object composition. Only spatial frequencies on the Ewald sphere are accessible to the imaging process, limiting attainable resolution.

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## Diffraction limits to resolution





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$$R \approx 0.61 \lambda / NA$$
 DOF ≈ 1.22 λ / (NA)<sup>2</sup> = 2 R<sup>2</sup> / (0.61λ)

 $|n| \approx 1 \Rightarrow NA << 1 \Rightarrow DOF << R$ 

### Synthesize larger NA with multiple views



**Cannot improve R, only DOF by tomography** 



1 Record many projections through sample over wide angular range. Projections at angles *q* contain:

$$I(x, y, \theta) = I_0 e^{-\int \mu_{\theta}(x', y', z') dz'}$$

2 Reconstruct 3D sample density from suite S of projections

Invert 
$$S\{I(x, y, \theta)\} \Rightarrow \mu(x, y, z)$$

## X-ray microscopy methods





Scanning x-ray microscopy/tomography



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Scanning nanotomography of chips





the second seco

Scanning transmission x-ray micrograph (1830 eV) of a Cu/W/Si test device, showing interconnects and vias.

Bayesian reconstruction reconstruction of 13 STXM projections (±69°, 1573 eV) through twolevel Al/W/Si test object. Al interconnects are joined by W vias. Two FIB markers are at top.

Z. Levine et al., Appl. Phys. Lett. 74, 150 (1999)

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Normal-incidence scan of interconnect showing electromigration void detail.

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Bayesian reconstruction of ragged end of void

Z. Levine, et al., J. Appl. Phys. 87, 4483 (2000)





## Detailed study of electromigration void



## Quantitative phase tomography

- Defocus series (a, b, c) and phase (d) of a silicon AFM tip
- Quantitative 3D reconstructions of real part of refractive index from ±70° tomographic projections through tip
- Calculated  $\delta$  = 5.1 x 10<sup>-5</sup> Measured  $\delta$  = 5.0 ± 0.5 x 10<sup>-5</sup>







P. McMahon et al., Opt. Commun. 217, 53 (2003)







Approaching the limit for focusing x-rays?

Kang et al., Phys. Rev. Lett. 96, 127401 (2006)

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Achieving high NA is challenging because x-rays interact weakly

 $n = 1 - \delta - i\beta$   $\delta, \beta \sim 10^{-3}$  to  $10^{-6}$   $\Rightarrow$  |n| ≈ 1



Differential-aperture x-ray microscopy



### **3D** depth-resolved, white-beam Laue diffraction technique



### B. Larson, W. Yang, G. Ice, *Nature* 415, 887 (2002)

## Studying 3D AI structure by DAXM





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- Resolution of real-space methods is fundamentally limited by optics technology. Because n ~ 1 for x-rays, NA << 1 and DOF << R (like electrons).</li>
- Reciprocal-space methods can benefit from high resolution detectors and optics ...
  - ⇒ But the resolution ultimately depends on neither. R and DOF are limited only by λ and usable signal.



- X-ray coherent diffraction is a *lensless* method suited for 3D imaging of non-crystalline structures
- Resolution limited only by measurable momentum transfer (NA)
- But: have phase problem full recovery is required, must assume some *a priori* information, e.g. object extent





**Record coherent diffraction pattern** 



- Phase information is obtained by measuring diffraction pattern at sufficiently fine intervals
- Reconstruct object amplitude by guessing at phase, then iteratively improving guess to get self-consistent solution
- Resolution: transverse R ~ 0.61 λ/NA
  longitudinal DOF ~ 1.22 λ/(NA)<sup>2</sup>
  - Contrast:  $\propto |f_1^2 + f_2^2|$





R. Gerchberg and W. Saxton, *Optik* 35, 237 (1972) J. R. Fienup, *Appl. Opt.* 21, 2758 (1982)

## **Biological objects**



Reconstructed coherent diffraction images of a freeze-dried yeast cell viewed at (A) normal, (C) 3°, and (D) 4° off-normal incidence. Labels identify the nucleus (N), a storage vacuole (V), and cell membrane (M). Image brightness represents magnitude, hue represents phase.

(B) STXM image taken of the same cell using 540-eV x-rays at ~42 nm resolution.



### D. Shapiro et al., PNAS 102, 15343 (2005)



- Optimizing contrast for biological specimens such as cytoskeletal actin filaments and mineralized fish bone
- Exploring resonant enhancement at absorption edges



Coherent diffraction pattern (2.2 keV) from a fish bone at a low mineralization state



Image of fish bone reconstructed solely from diffraction data

### J. Miao, C. Song (UCLA)



| Record hologram | $I =  a+b ^{2} =  a ^{2} +  b ^{2} + a^{*}b + ab^{*}$ |
|-----------------|---|
| Reconstruct     | $bI = b a ^{2} + b b ^{2} + a^{*}bb + abb^{*}$        |
|                 | $= aI_b + b(I_a + I_b) + background$                  |

- Reference wave encodes magnitude and phase of wave scattered by object in hologram
- Contrast and resolution: same as for coherent diffraction
- Reconstruct sample amplitude by "re-illuminating" hologram with reference wave (or its C.C.)

## Holography



D. Gabor, Nature 161, 777 (1948)

G. Stroke, *Appl. Phys. Lett.* 6, 201 (1965) Winthrop, Worthington, *Phys. Lett.* 15, 124 (1965)

![](_page_29_Picture_7.jpeg)

## FT hologram formation

![](_page_30_Picture_1.jpeg)

![](_page_30_Figure_2.jpeg)

object wave

reference wave

$$I = |a+b|^2 = |a|^2 + |b|^2 + a^*b + ab^*$$

### hologram intensity

![](_page_31_Picture_1.jpeg)

- Numerically take FT of hologram intensity to reconstruct
- Spatially separated primary, conjugate object waves result
- Weak curvature f(x,y) on object wave can be ignored

mage terms: 
$$a^*b+ab^* = \varphi(s\xi)F(\xi,\eta)+\varphi(s\xi)^*F(\xi,\eta)^*$$

where: 
$$F(\xi,\eta) = \frac{e^{ikz}}{i\lambda z} f(\xi,\eta) \iint a(x,y) f(x,y) e^{-\frac{ik}{z}(x\xi+y\eta)} dxdy$$
,

$$\varphi(s,\xi) = e^{-\frac{ik}{z}s\xi} \text{ and } f(\xi,\eta) = e^{\frac{ik}{2z}(\xi^2 + \eta^2)}$$
$$FT^{-1}\{a^*b + ab^*\} = f(x-s,y)a(x-s,y) + f(-(x-s),-y)^*a(-(x-s),-y)^*$$

## Hard disks: storage density

![](_page_32_Picture_1.jpeg)

![](_page_32_Figure_2.jpeg)

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CoPt magnetic labyrinth nanostructures

![](_page_33_Picture_1.jpeg)

side view

![](_page_33_Figure_3.jpeg)

Sample: O. Hellwig (Hitachi)

MFM, top view

![](_page_33_Picture_6.jpeg)

 $5 \ \mu m \ x \ 5 \ \mu m$ 

continuous object

SiN<sub>x</sub> / Pt (24 nm) / [Co (1.2 nm) / Pt (0.7 nm)]<sub>50</sub> / Pt (1.5 nm)

perpendicular anisotropy

→ magnetic storage media

### Pinhole mask method

![](_page_34_Picture_1.jpeg)

![](_page_34_Figure_2.jpeg)

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![](_page_35_Picture_0.jpeg)

**STXM** 

### FTH

![](_page_35_Figure_2.jpeg)

Switching in patterned magnetic media

![](_page_36_Picture_1.jpeg)

#### LETTERS

![](_page_36_Picture_3.jpeg)

Ø 110 nm

![](_page_36_Figure_5.jpeg)

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16 June 2006

Z. Xiao et al., J. Am. Chem. Soc. 126, 2316 (2004)

## Nanostructure of multi-twinned crystals

- Multi-twinned Pb crystals >5 µm in size are readily grown by electrodeposition. Morphology is strongly dependent on the electrochemical potential
- Calculations indicate they should not grow larger than ~200 nm due to strain near grain boundaries
- Even highly regular "crystals" show little or no Bragg diffraction
- If crystals, what is their structure, orientation, and nature of defects?
- Are they amorphous? If so, how do they grow?

![](_page_37_Picture_9.jpeg)

![](_page_37_Picture_10.jpeg)

![](_page_38_Picture_1.jpeg)

![](_page_38_Figure_2.jpeg)

- Beam passing through zone plate (0th-order) illuminates sample.
- Beam focused by zone plate (3rd-order) serves as reference. Reference wave interferes with object wave to form hologram.
- NA of reference wave determines hologram resolution. Detector resolution determines object field of view.

## Sample

![](_page_39_Picture_1.jpeg)

![](_page_39_Picture_2.jpeg)

### Y. Xiao (APS), Z. Xiao (ANL/MSD)

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## Holograms

![](_page_40_Picture_1.jpeg)

![](_page_40_Figure_2.jpeg)

### Only part of hologram recorded

- limit direct-beam blooming
- increase angular resolution
- collect un-phased diffraction

### ... but pay penalty:

 much sample information not recorded, especially at lowest spatial resolution

![](_page_41_Picture_1.jpeg)

![](_page_41_Picture_2.jpeg)

3 µm

Closeup SEM of Pb crystal. Crystal is ~4.5 µm in extent; dendrites are 100-300 nm wide. Reconstructed FT hologram. Field of view is limited to  $\sim$ 5 µm by detector resolution. X-ray energy was 1050 eV.

![](_page_42_Picture_0.jpeg)

![](_page_42_Picture_1.jpeg)

#### Magnitude

Phase

phase = 
$$\tan^{-1} \left\{ \frac{\operatorname{Im}(\psi)}{\operatorname{Re}(\psi)} \right\}$$

Coherent diffraction is aided by Fresnel

![](_page_43_Picture_1.jpeg)

### G. Williams, K. Nugent (U. Melbourne)

![](_page_43_Picture_3.jpeg)

## Fresnel diffraction imaging

![](_page_44_Picture_1.jpeg)

![](_page_44_Picture_2.jpeg)

![](_page_44_Picture_3.jpeg)

Phase

Magnitude with color-encoded phase

## 3D coherent diffraction microscopy

![](_page_45_Picture_1.jpeg)

![](_page_45_Picture_2.jpeg)

(a) SEM of pyramidal indentation in a 100-nm  $Si_3N_4$  membrane lined with 50-nm Au spheres. (b) 3D image reconstructed from 123 diffraction projections spanning -57° to +66°, using reality and positivity constraints. (c) Large DOF projection. (d) Enlarged region of (c).

H. Chapman et al., J. Opt. Soc. Am. A23, 1179 (2006)

## 3D coherent diffraction microscopy

![](_page_46_Picture_1.jpeg)

![](_page_46_Figure_2.jpeg)

(a) SEM of pyramidal indentation in a 100-nm  $Si_3N_4$  membrane lined with 50-nm Au spheres. (b) 3D image reconstructed from 123 diffraction projections spanning -57° to +66°, using reality and positivity constraints. (c) Large DOF projection. (d) Enlarged region of (c).

H. Chapman et al., J. Opt. Soc. Am. A23, 1179 (2006)

![](_page_47_Picture_1.jpeg)

### **Technically challenging**

- Precision sample rotation and targeting in x,y,z
- Short working distance at high NA (using optics)
- Radiation dose to sample (but Dose fractionation helps)

### **Physical limitations restrict**

- Accessible angular range
- Number of views obtainable
- Sample field-of-view

### ... time consuming!

### ⇒ Parallelize projection acquisition

Multi-view holography with beamsplitter

![](_page_48_Picture_1.jpeg)

![](_page_48_Figure_2.jpeg)

Possible method for one-shot tomography. Six holograms are shown but they are part of a 2D array of 7x7-1 = 48

## Multiple illumination directions

![](_page_49_Picture_1.jpeg)

![](_page_49_Figure_2.jpeg)

![](_page_49_Picture_3.jpeg)

Micromachined Si mirror nanoactuators for x-ray astronomy

M. Schattenberg, MIT

Parallel tomographic coherent diffraction. N beams are directed through sample onto N detectors

![](_page_50_Picture_1.jpeg)

- Coherent diffraction microscopy is getting easier, but phase retrieval is slow and uniqueness problem not solved.
- Holograms are quickly and reliably reconstructed in seconds on a small computer. Pinholes give cleanest results, but ZPs are best for sample and scalable to hard x-rays. Holographic data aids diffraction phase recovery.
- Currently takes ~10<sup>10</sup> photons for ~50 nm resolution (2D). ERL should provide enough coherent flux for 3D data set at same resolution and in same time.

## Snapshots: smaller & faster

![](_page_51_Picture_1.jpeg)

### Stanford 1878

![](_page_51_Picture_3.jpeg)

## One day ... ps magnetic imaging?

![](_page_52_Picture_1.jpeg)

![](_page_52_Figure_2.jpeg)

### J. Stohr (Stanford U.)

![](_page_53_Picture_1.jpeg)

- X-ray microscopy is now being used to image nanoscale 3D structures at 3rd-generation sources, but acquisition takes days.
- Coherent diffraction avoids optics limitations and can be combined with tomography for 3D imaging. Parallel data collection will enable time-resolved studies.
- Materials science at the nanometer scale, especially time-resolved problems, will benefit from the 1000x higher brilliance of the ERL.

![](_page_54_Picture_1.jpeg)

Stefan Eisebitt, Chris Günther, Andreas Menzel, Florin Radu

Lixin Fan, Yanan Xiao

**David Paterson** 

Jianwei Miao, Changyong Song

Keith Nugent, Andrew Peele

**Bill Schlotter** 

Olaf Hellwig

BESSY

**Advanced Photon Source** 

Australian Synchrotron

U. California at Las Angeles

University of Melbourne

**Stanford University** 

Hitachi Almaden Res. Center

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